

# Prediction Of Diabetic Retinopathy With Pyramidal Structured Convolution And Rank-Based Lesion Candidate Estimation

Mrs. Sharmila EMN<sup>1</sup>, Dr. Prof. R. Suchitra<sup>2</sup>

<sup>1</sup>Research Scholar, Chirashree Institute of Research and Development & RPA First Grade College, (Approved by University of Mysore)

Email Id-[emnsharmila@gmail.com](mailto:emnsharmila@gmail.com)

<sup>2</sup>Professor & Research Guide, Chirashree Institute of Research and Development & RPA First Grade College, (Approved by University of Mysore)

Email Id-[suchithra.suriya@gmail.com](mailto:suchithra.suriya@gmail.com)

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## Abstract

*This paper proposes a diabetic retinopathy (DR) grading approach that uses pyramidal structured convolution (Py-CNN) with a rank-based lesion candidate estimation process for extracting the deep lesion descriptors. Initially, the proposed approach segments the possible lesion candidates after preprocessing using the HSV transform-based adaptive histogram equalization approach. The top  $K$  segmented lesion candidates are ranked based on the edge and energy components present in the lesion candidates. The pyramidal structured convolution has different sections of the convolutional filter where each section processes the ranked lesion candidates. The lower section of the pyramidal structured convolution has higher length filters that process the top-ranked lesion candidates. The length of the convolutional filter reduces as the rank of the lesion candidate reduces. Two networks namely Network-A and Network-B are utilized to extract the global fundus image and deep lesion candidature descriptors. The deep lesion candidature descriptors are implanted in the lesion region of the feature map with the use of a diffusion layer. The diffused descriptors are used by one of the dense networks, while the global descriptors and the deep lesion candidature descriptors are used by another dense network. Based on the predicted probability of the two dense networks the actual classification result can be computed. Datasets namely APTOS 2019 and Messidor-2 are utilized to evaluate the algorithm performance with different evaluation scales. The proposed approach results in a specificity, Mathew's correlation coefficient, F1-score, precision, and accuracy of 99.36%, 96.77%, 97.41%, 97.35%, and 97.47% when evaluated using the APTOS 2019 datasets.*

**Keywords:** Diabetic retinopathy, Severity grading, Convolutional neural network, Dense network, Lesion candidates.

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## 1. INTRODUCTION

The primary cause of vision loss in diabetes patients across the globe is diabetic retinopathy (DR) [1]. This DR has early symptoms such as a dark area in vision, blurred vision, vision spots, and progressive loss of vision [2]. The stages of DR include non-proliferative phases (NPDR) such as mild, moderate, and severe. The stage after the non-proliferation leads to the

proliferative phase (PDR). The mild NPDR is the early stage where small bulges occur in the blood vessel. At the moderate NPDR stage, the retina gets damaged with the formation of hard exudates, retinal hemorrhages, and microaneurysms. Severe NPDR is the advanced stage in the NPDR phase where abnormal blood vessel growth occurs with the formation of extensive microaneurysms, and hemorrhages [3]. The advanced stage DR is PDR where there is extensive growth of blood vessels. Ophthalmologists assess the DR grade on fundus images based on factors such as width, color, angle, and length. The manual detection of DR severity grades is prone to errors and can utilize more time [4]. Different authors proposed different schemes for grading the DR levels in which the deep learning approach plays a vital role. Even though optical coherence tomography (OCT) [5] imaging provides cross-sectional information, the fundus imaging-based diagnosis is low-cost and low time-consuming.

The authors Wan et al. [6] used convolutional neural networks (CNN) along with hyperparameter tuning, and transfer learning [7] approaches. Transfer learning approaches namely ResNet, GoogleNet, VggNet, and AlexNet are utilized in the classification model. An ensemble scheme was proposed [8] which uses five different deep models such as Dense169, Dense121, exception, inceptionV3, and ResNet50. This deep model improves the performance in DR classification by extracting effective descriptors from fundus images. Capsule network [9] is used along with convolutional filters to extract fundus image features. This approach also uses a soft-max layer, and class capsule layer to detect the severity class of the fundus image. The authors Kar et al. [10] detected the DR levels in four stages. Initially, the optic disc present in the fundus image is removed and the vessels are extracted. The resultant image is pre-processed, and the lesion candidates are detected. Finally, the false candidates are eliminated in the post-processing stage. To eliminate the regions that are poorly illuminated a curvelet edge enhancement process is utilized. To identify the DR level and suspicious regions, attention maps are generated to derive a zoom-in-net approach [11]. For classification, this approach not only uses the suspicious patches it also considers the complete retinal image. The computation of this zoom-in process is high, though it provides reasonable performance.

The CNN algorithm [12] is used to detect the occurrence of microaneurysms [13], in which the affected and normal regions are categorized using semantic segmentation. Based on the semantic segmentation results, the segmented region is trained to classify the NPDR severity levels. To improve the ability of feature extraction Calvin et al. [14] modify the VGG-16 model to derive attention-enhanced VGG-16 architecture. Spatial and channel attention are also utilized to obtain the relational descriptors. CNN with squeeze and excitation framework is utilized to identify the dominant descriptors and channels. This approach also uses a DeepRetiNet for separating the hard exudates. Crossover grasshopper scheme [15] was used to improve feature extraction. This approach combines the optimization algorithm, and the deep learning model to collect essential descriptors from the fundus pictures. Further, a generative adversarial network (GAN) is used for feature augmentation which uses a multi-class classifier instead of a binary classifier. Due to the deployment of optimization algorithms in the deep learning model, the complexity is higher.

Roberto et al. [16] used attention to separate the bright and dark structures of the retina. This attention focuses on hard exudates, hemorrhages, and microaneurysms. To handle the data imbalance problem a focal loss function is used while the descriptors are extracted with Xception architecture. This scheme provides a Kappa of 0.78, and an accuracy of 83.7% which can be further improved. A capsule network [17] is used along with a vision transformer for predicting the DR severity. Initially, contrast limited adaptive histogram equalization (CLAHE) is used along with power

law transform as pre-processing. The usage of capsule networks in the tuned vision transformer yields an accuracy of 87.78% in the Messidor-2 dataset. The principal component analysis [18] is used to extract the descriptors from the pre-processed fundus images. Deep features are also extracted utilizing the pre-trained CNN structures namely SqueezeNet, ResNet152, and ResNet150. Usage of the pre-trained model ResNet152 yields a maximum accuracy of 94.4% in the APTOS 2019 dataset.

For segmenting the blood vessels, and optic disc the author Zhu et al. [19] proposed the independent U-Net structures. The inceptionV3 model is used to extract the feature, while the features are classified using the symmetric CNN with singular value decomposition (CNN- SVD) structure. During the backpropagation stage of CNN, a synaptic metaplasticity [20] process is used that also uses inceptionV3 structures for feature extraction. This approach provides an F1-score of 94.24% with reduced complexity. A radial basis function classifier

[21] is used to classify DR and non-DR in which features are extracted from microaneurysms, exudates, and blood vessels which are detected by the Histon-based segmentation process. Bi-channel CNN was proposed by Lin et al. [22], where the green component is utilized to estimate the entropy, and unsharp masking for enhancing the fundus image. The bi-channel CNN classifies the fundus image using the green component, and grey level image. To compensate for the non-uniform brightness in the fundus image, the authors Tamoor et al. [23] used modified gamma correction and a Gaussian match filter. Further, mathematical morphology and entropy thresholding are used to detect the lesion candidates from which the candidate descriptors are extracted by shallow models like AlexNet, and LeNet-5. The red lesions are detected [24] for classifying the DR, and non-DR in fundus images. Two CNN models are utilized to extract the features and to perform DR classification.

The DR grading approaches that are discussed above do not use a rank-based lesion candidate deep descriptor extraction process. The rank-based lesion candidate extraction process will extract more deep descriptors from the lesion candidates that contribute more to DR grading. Moreover, the descriptors are extracted from these lesion candidates based on the estimated rank. This deep descriptor which is extracted from the lesion candidates along with the global descriptor is utilized to classify the DR types. The key contribution of the work is highlighted below.

- (i) The work proposes a pyramidal structured convolution-based DR grading approach that estimates the lesion candidates from which the candidate rank is computed. The pyramidal structural convolution will extract the descriptor based on the rank of the lesion candidate.
- (ii) The work also proposes a feature diffusion process, which implants the feature maps of the lesion candidates on the feature map that represents the global descriptor.
- (iii) The work uses two dense networks for classifying the feature where the first network predicts the class probability using the global and the deep descriptor extracted from the lesion candidates, while the second network predicts the class probability using the diffused feature map descriptor.
- (iv) Finally, the evaluation of the suggested Py-CNN-based DR grading was done based on the average of the predicted probability result obtained from the two dense networks. Datasets Messidor-2 and APTOS 2019 are utilized in the evaluation of the Py-CNN model-based DR grading in classifying 5 different DR severity grade levels.

The description of the forthcoming sections is summarized as follows. Section 2 explains the proposed Py-CNN-based DR grading approach along with its architecture. Section 3 provides the analysis of the Py-CNN approach and lastly, the conclusion is presented in Section 4.

## 2. PROPOSED METHOD

The suggested Py-CNN-based DR grading approach involves major steps such as Fundus image preprocessing, detection of lesion candidate, Edge, and energy-based DR ranking, and Py-CNN classifier as provided in Fig. 1.

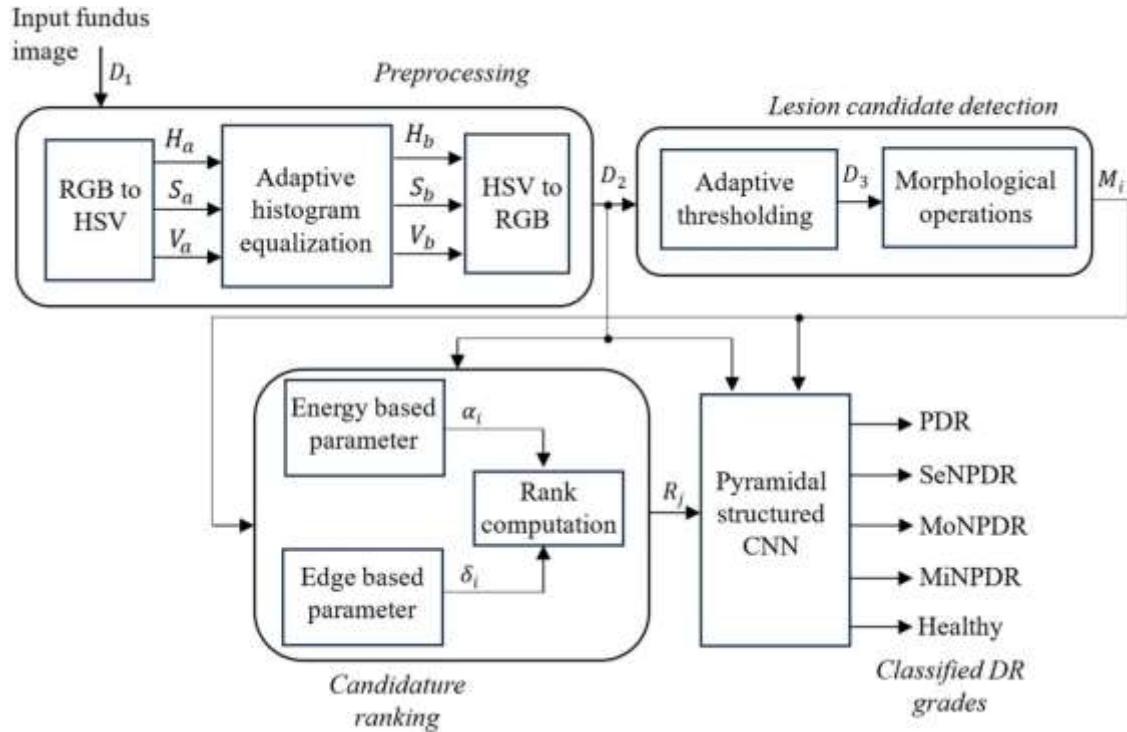


Fig.1:StructureofthesuggestedPy-CNN-basedDRseveritygradingapproach

#### (a) Fundusimagepreprocessing

ThepreprocessinginthesuggestedPy-CNN-basedDRgradingapproachaimstoenhancethe lesion candidate region suitable for segmentation since the lesion candidate regions are utilized to extract the deep candidate descriptors. Let  $D_1$  resembles the input fundus picture. This includesresizingtheimagetoadimensionof  $256 \times 256$ , medianfiltering, andenhancingthe image by HSV and CLAHE-based approach [25].The approach initially converts the RGB funduspicturetoHSVcoefficients  $(H_a, S_a, V_a)$ , andeachcoefficientisenhancedusingthe CLAHEapproach.Aftertheenhancementofeachchannel, theenhancedHSVcoefficients  $(H_{b,b}, V_{b,b})$ , areagainconvertedbacktoRGBformtoobtaintheenhancedfunduspicture  $D_2$ .

#### (b) Detectionoflesioncandidate

Let  $D_2$  resemble the pre-processed image in which the DR lesion candidates are enhanced. The lesion candidates are then detected from this image  $D_2$  by the processes such as adaptive thresholding and morphological operations. Since the DR lesion candidates have darker intensity than other regions, the adaptive thresholding [26] will segment the lesion candidates whose adaptive threshold is less than  $(x, y)$  which varies throughout the fundus picture. The lesion candidates can be detected by the relation

$$D_3(x,y)= \begin{cases} 1 & \text{if } (x,y) < \lambda(x,y) \\ 0 & \text{otherwise} \end{cases} \quad (1)$$

The segmented picture  $D_3(x,y)$  also contains small noisy structures. Thus, small objects (connected regions) whose area is less than 30 pixels are not considered. Further erosion is performed so that the blood vessels further shrink. For erosion, a disk structuring element with a radius of 1 is used. Again, the small objects whose area is less than 30 are further eliminated which removes the blood vessels. From the resultant objects, dilation is performed to obtain the boundaries of the lesion region. For dilation, a disk structuring element with a radius of 2 is used. Let the segmented lesion candidate picture contain  $\beta$  number of lesion candidates represented as  $M_i$ , where  $i = 1, 2, \dots, \beta$ .

### (c) Edge and energy-based DR ranking

In the edge and energy-based DR ranking approach, the lesion candidates are ranked by estimating the energy and edge parameters. The lesion region usually has higher energy and edge information. Thus top  $K$  lesion candidates that have higher ranks are utilized to extract deeper descriptors. This deep descriptor is extracted by the parallel sections of the Pyramidal structured convolutional filter. From  $\beta$  number of lesion candidates represented as  $M_i$ , top  $K$  lesion candidates are selected which is represented as  $\hat{M}_j$  where  $j = 1, 2, \dots, K$ . Let the energy variation of each candidate be  $\alpha_i$  which can be estimated by the expression,

$$\alpha_i = \rho_i - \mu \quad (2)$$

Here  $\rho_i$  and  $\mu$  resembles the energy of the lesion candidate and background respectively. The energy parameter  $\alpha_i$  gives the energy variation between the lesion candidate and background respectively. Let  $s_1$  resemble the number of pixels in the fundus image. The average energy of the background region can be expressed as

$$\mu = \frac{1}{s_1} \sum_{(x,y) \in R} ((x,y))^2 \quad (3)$$

Here  $R$  resembles the complete fundus image region. Similarly, the average energy of the lesion candidate region  $M_i$  can be estimated as

$$\rho_i = \frac{1}{\gamma_i} \sum_{(x,y) \in M_i} ((x,y))^2 \quad (4)$$

Here  $\gamma_i$  resembles the number of pixels enclosed in the lesion candidate region  $M_i$ . Substituting the average energy of the lesion candidate and the background region in equation (2), the energy parameter can be expressed as,

$$\alpha_i = \frac{1}{\gamma_i} \sum_{(x,y) \in M_i} ((x,y))^2 - \frac{1}{\gamma_i} \sum_{(x,y) \in R} (D(x,y))^2 \quad (5)$$

The edge parameter  $\delta_i$  can be computed for each lesion candidate region  $M_i$  by subtracting the smoothened components of the lesion candidates. Thus, the edge information can be estimated as

$$\delta_i = \frac{1}{\gamma_i} \sum_{(x,y) \in M_i} (D(x,y) - \bar{D})^2 \quad (6)$$

Here  $(x,y) \in M_i$ . From the edge information, the edge parameter can be computed as

$$\delta_i = \frac{1}{\gamma_i} \sum_{(x,y) \in M_i} ((x,y))^2 \quad (7)$$

The edge parameter gives the average energy of the edges. The energy parameter  $\alpha_i$  and the edge parameter  $\delta_i$  are used to compute the ranking parameter  $r_i$ , which can be estimated from the sum of the edge parameter and the energy parameter

$$r_i = \delta_i + \alpha_i \quad (8)$$

The ranking parameter is sorted in descending order and the lesion candidates that have top  $K$  ranking parameter values are selected for extraction of deep features. Let the index of the lesion candidates that have top  $K$  ranks be  $R_j$ . The selected top- $K$ -ranked lesion candidates are utilized to extract the deep features by the pyramidal-structured convolutional filters.

#### (d) Py-CNN classifier

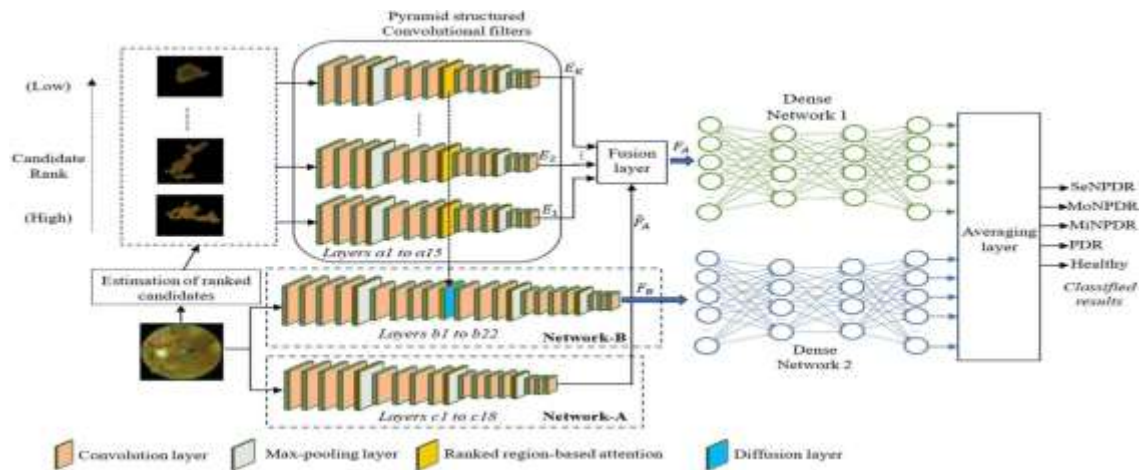
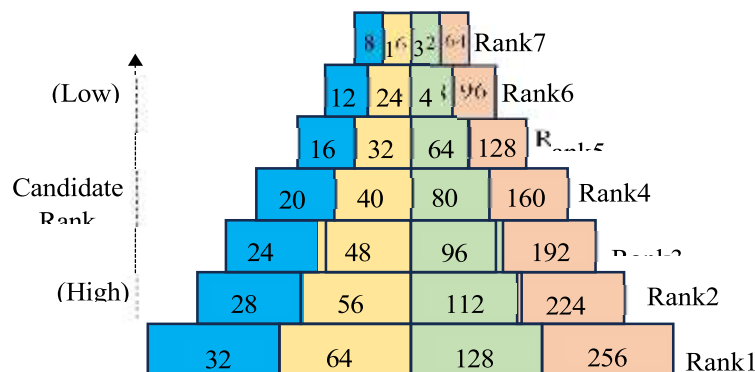


Fig.2:Architecture of suggested Py-CNN classifier used in proposed DR grading approach

The structure of the Py-CNN classifier in detecting the DR grade levels is provided in Fig. 2. Three different features are extracted by the Py-CNN classifier namely the global feature, deep lesion candidate features, and the diffused feature. These three features are utilized by two dense networks to classify the DR grade levels. Two subnetworks namely Network-A and Network-B are utilized in the suggested Py-CNN. The pyramidal structured CNN has different sections of convolutional filters, where the lesion candidates corresponding to different ranks are processed by each section. The bottom section corresponds to top-ranked lesion candidates, while the top section corresponds to the low-ranked lesion candidates. Thus, the bottom section of the pyramidal structured filter will have convolutional filters that have higher lengths (more channels), while the top section of the pyramidal structured filter will have convolutional filters with a lower length (few channels). The filter length used by the pyramidal structured filter with 7 sections are illustrated in Fig. 3. The pyramidal structured filter with 7 sections resemble that, top-7 lesion candidates are utilized to extract the deep lesion descriptors. In this pyramidal filter, the filter length (channel) reduces as rank reduces.



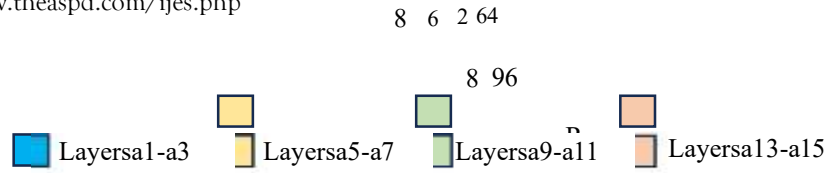


Fig.3:Representation of pyramidal structure convolutional length used in Py-CNN

The input to the Py-CNN includes the mask of lesion candidates  $M_j$  that have top  $K$  ranks  $R_j$  along with the fundus image that was preprocessed i.e.  $D_2(x, y)$ . The lesion candidates are segmented using the mask and resized with a fixed dimension of  $64 \times 64$ . The description of various layers used in the Py-CNN is provided in Table I. The layers  $a1$  to  $a3$ ,  $5$  to  $a7$ ,  $a9$  to  $a11$ , and  $a13$  to  $a15$  in Py-CNN architecture have a size of  $64 \times 64$ ,  $32 \times 32$ ,  $16 \times 16$ , and  $8 \times 8$  respectively. The number of channels used by the filters in the pyramidal convolutional section is provided in Fig. 3.

Table I: Specification of layers (Network-A and Network-B) used in Py-CNN

Layers	Description	Output size
$b1$ to $b4$	$5 \times 5, 32, \text{stride-1}$	$256 \times 256$
$b6$ to $b13$	$5 \times 5, 64, \text{stride-1}$	$128 \times 128$
$b15$ to $b18$	$3 \times 3, 128, \text{stride-1}$	$64 \times 64$
$b20$ to $b22$	$3 \times 3, 256, \text{stride-1}$	$32 \times 32$
$c1$ to $c4$	$3 \times 3, 32, \text{stride-1}$	$256 \times 256$
$c6$ to $c9$	$3 \times 3, 64, \text{stride-1}$	$128 \times 128$
$c11$ to $c14$	$3 \times 3, 128, \text{stride-1}$	$64 \times 64$
$c16$ to $c18$	$3 \times 3, 256, \text{stride-1}$	$32 \times 32$

The max-pooling layer uses a filter size of  $2 \times 2$ , and stride-1. Apart from convolutional layers and max-pooling layers, the Py-CNN also has ranked region-based attention and diffusion layers. The ranked region-based attention will eliminate the feature outside the region of interest represented by the scaled mask ( $32 \times 32$ ) which has two outputs. One of the outputs is used by the succeeding layers of the same section, while the other output is used by the diffusion layer after resizing to the size of the scaled mask in Network B. The ranked region-based attention performs functions such as eliminating the features outside the region of interest, multiplication by the ranking weight, and max-pooling as illustrated in Fig. 4.



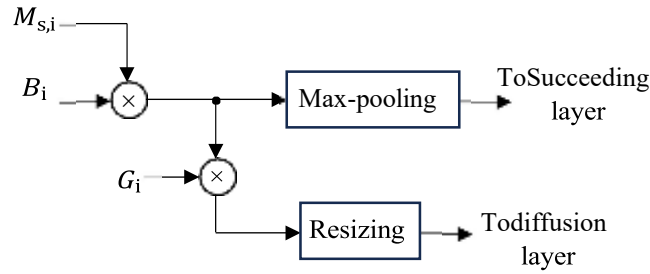


Fig.4:Representation of rank-based attention layer used in Py-CNN

Let the scaled mask image be represented as  $M_{s,i}$  and the feature map obtained from the previous layer be  $B_i$ . Let  $G_i$  be the weight that is used by the rank-based attention. The weights of the rank-1 to rank-7 lesion candidates are assigned as  $G_i = [1, 0.9, 0.8, 0.7, 0.6, 0.5, 0.4]$ .

The succeeding layers of the pyramidal section use the max-pooled output of  $M_{s,i}B_i$ , while the

network-B or diffusion layer uses the resized lesion candidate region of  $M_{s,i}B_iG_i$ . The diffusion layer implants the attention layer output in its corresponding lesion candidate region using its scaled mask  $M_{s,i}$ . Before implanting the feature, the attention output  $M_{s,i}B_iG_i$  is resized to a size suitable for diffusion. During the diffusion, the feature maps of the diffusion layer has a larger filter length than the rank-based attention layer. For example, the layer before the diffusion layer in network B has a length of 64, but the output from the pyramidal filter section (rank-2) has a length of 56. Thus, the first 56 feature map of the diffusion layer corresponding to the region of the lesion candidate is replaced by the feature map from the first 56 attention layers, while the remaining feature maps (56 to 64) of network-B are unchanged.

The output of network-A and network-B is represented as  $\hat{F}_A$  and  $F_B$ . The feature  $\hat{F}_A$  is termed to be a global descriptor obtained from a complete fundus image and feature  $F_B$  is termed to be a diffused descriptor. The features obtained from each section of the lesion candidates (Top- $K$ ) be represented as  $E_1, E_2, \dots, E_K$ . The global descriptor  $\hat{F}_A$  and the lesion candidate descriptor  $E_1, E_2, \dots, E_K$  can be combined to obtain the feature to be trained by dense layer-1. Thus, the input feature to dense layer-1 can be estimated as

$$F_A = [\hat{F}_A, E_1, E_2, \dots, E_K] \quad (9)$$

The dense network 1 and dense network 2 use the flattened version of the feature  $F_A$  and  $F_B$  respectively. The dense network 1 and convolutional filters of network A use the following (equation (10)) cross-entropy loss function to update the kernels and weights in the dense network 1.

$$Q_C = - \sum_z \mathbf{a}_z \log \hat{\mathbf{a}}_z \quad (10)$$

Here,  $\hat{\mathbf{a}}_z$  resembles the predicted probability for class  $z$  from dense network 1, while  $\mathbf{a}_z$  is the actual probability and  $z$  is the number of classes. The dense network 2, pyramidal filter section, and the

convolutional filters in network-B use the loss function expressed as

$$Q = \frac{1}{L_{tr}} \sum_{l=1}^m (b - \hat{b})^2 \quad (11)$$

Here,  $L_{tr}$  resembles the number of images used in training,  $b$  resembles the actual probability

of  $l^{th}$  training image,  $\hat{b}$  resembles the predicted probability of the  $l^{th}$  image. The convolutional filters and the dense network update the weights using the respective loss function  $Q \in \{Q_{c,m}\}$  with the following weight update equation

$$h(t+1) = h(t) - 5 \frac{dQ}{dh} \quad (12)$$

Here  $h(t)$  and  $h(t + 1)$  resembles the past weight and the updated weight respectively at iteration  $t$  with learning rate 5. The proposed approach uses ReLu activation after each convolutional filter. From the predicted probability of the two dense networks (dense network 1 and dense network 2), the actual output can be computed from the average of the two dense network probabilities.

### 3. EXPERIMENTAL RESULTS

The fundus image datasets namely Messidor-2 [27] and APTOS 2019 [28] are utilized to evaluate the Py-CNN-based approach. The evaluation measures namely, F1-Score, Recall, Specificity, Precision, Accuracy, and Mathew's correlation coefficient (MCC) are utilized to evaluate the Py-CNN-based approach. The evaluation parameter can be evaluated using the relations provided below,

$$F1-Score = \frac{\Delta_{tp}}{\frac{1}{2}(\Delta_{fn} + \Delta_{fp}) + \Delta_{tp}} \times 100\% \quad (13)$$

$$Recall = \frac{\Delta_{tp}}{\Delta_{fn} + \Delta_{tp}} \times 100\% \quad (14)$$

$$Specificity = \frac{\Delta_{tn}}{\Delta_{tn} + \Delta_{fp}} \times 100\% \quad (15)$$

$$MCC = \frac{\Delta_{tp} \times \Delta_{tn} - \Delta_{fp} \times \Delta_{fn}}{\sqrt{(\Delta_{tp} + \Delta_{fp}) \times (\Delta_{tp} + \Delta_{fn}) \times (\Delta_{tn} + \Delta_{fp}) \times (\Delta_{tn} + \Delta_{fn})}} \times 100\% \quad (16)$$

$$Precision = \frac{\Delta_{tp}}{\Delta_{tp} + \Delta_{fp}} \times 100\% \quad (17)$$

$$Accuracy = \frac{\Delta_{tp} + \Delta_{tn}}{\Delta_{tp} + \Delta_{tn} + \Delta_{fp} + \Delta_{fn}} \times 100\% \quad (18)$$

Here,  $\Delta_{tn}$ ,  $\Delta_{fp}$ ,  $\Delta_{fn}$ , and  $\Delta_{tp}$  be the true negative, false positive, false negative, and true positive result estimated in the testing phase of the proposed Py-CNN-based approach. DR grades namely severe NPDR (SeNPDR), mild NPDR (MiNPDR), moderate NPDR (MoNPDR), PDR, and Healthy classes are utilized for evaluating these severity level. The number of images utilized from the Messidor-2 and APTOS-2019 datasets are listed in Table II. Out of 999 images, only 500 images are randomly selected for the class MoNPDR from the APTOS 2019 dataset.

Table II: Number of images utilized for analyzing the suggested Py-CNN-based DR classification approach (Here \* resembles the class in which augmentation is not performed)

Augmentation	Dataset	SeNPDR	MoNPDR	MiNPDR	PDR	Healthy*
Before	APTOS2019	193	500	370	295	1805
	Messidor-2	75	347	270	35	1017
After	APTOS2019	1158	3000	2220	1770	1805
	Messidor-2	450	2082	1620	210	1017

Table II also shows the number of images after augmentation. Five different augmentations namely 3 rotations (90°, 180°, 270°), brightening, and darkening by 50 are used. Using the augmented images, 30% of images are randomly chosen for classification, while the remaining 70% of images are utilized for training. The distribution of training and testing images in each class is provided in Fig. 5.

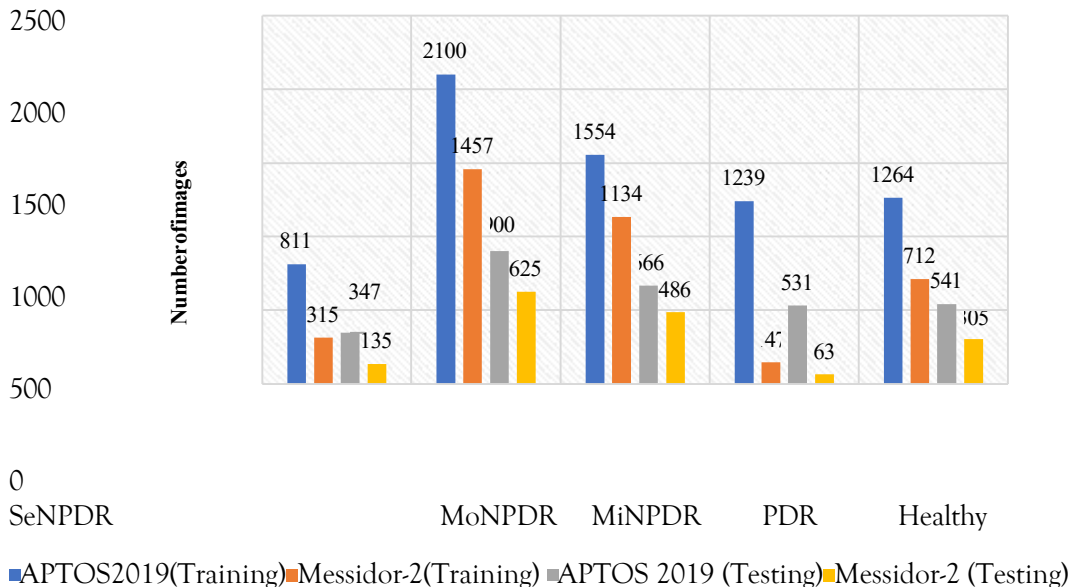


Fig. 5: Distribution of training and testing data used for the analysis of the suggested Py- CNN-based

approach

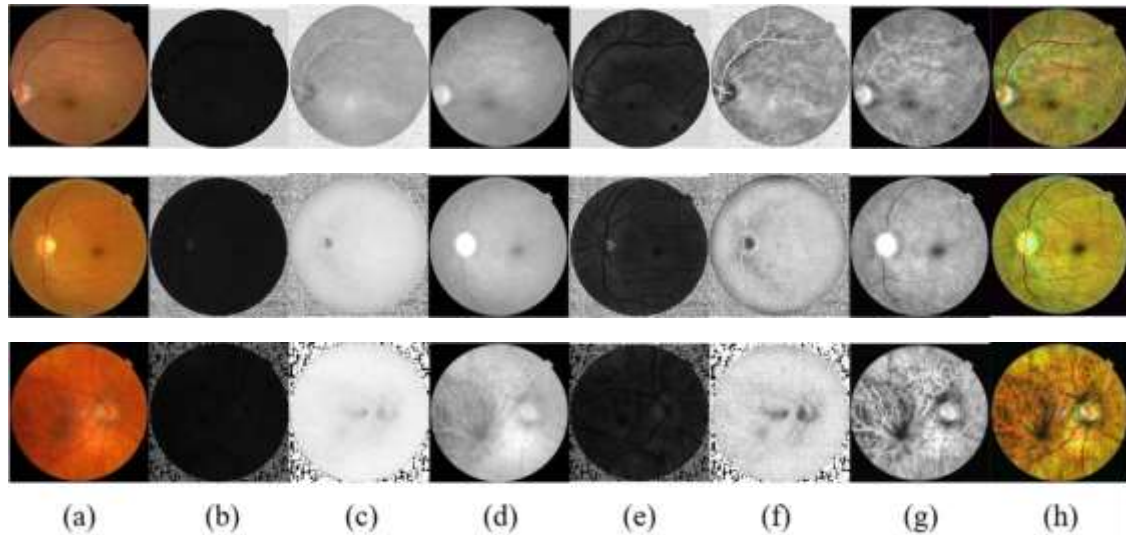
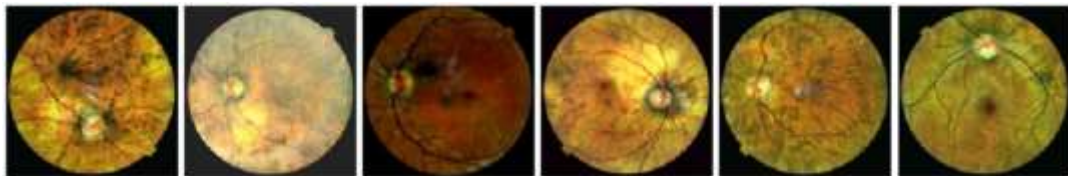


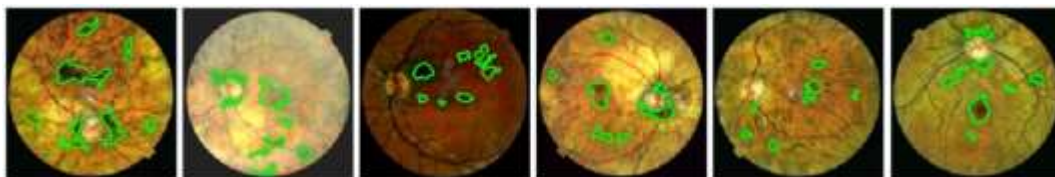
Fig. 6: Preprocessing result obtained in the suggested scheme (a) Input fundus picture (b)-components (c)  $S$ -components (d)  $V$ -components (e) CLAHE enhanced  $H$ -component (f) CLAHE enhanced  $S$ -component (g) CLAHE enhanced  $V$ -component (h) Pre-processed fundus picture

The preprocessing result obtained by the suggested Py-CNN-based approach is depicted in Fig.

6. The CLAHE algorithm enhances all three components ( $H, S, V$ ) to obtain the enhanced image. The optical disc, blood vessels, and microaneurysms are clearly visible in the pre-processed picture. The CLAHE scheme utilizes a grid size of  $8 \times 8$  and a clip limit of 40.



(a)



(b)

Fig. 7: Representation of top-7 ranked lesion candidates estimated in the Py-CNN-based approach (a) Input image (b) Top-7 lesion candidates

The top-7 ranked lesion candidates selected by the energy and edge parameter-based ranking are illustrated in Fig. 7. These top-7 ranked lesion candidates are utilized to extract deep lesion candidate descriptors if the  $K$  value is chosen as 7.

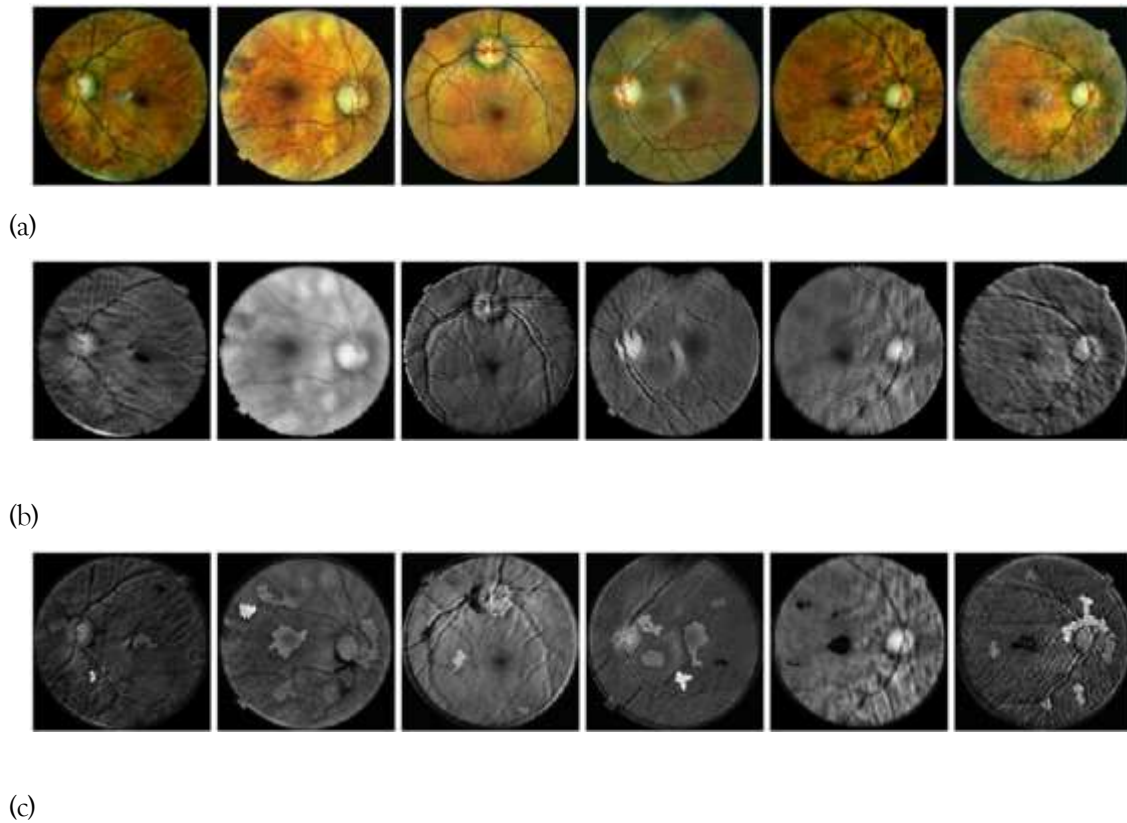


Fig. 8: Feature maps obtained by the trained convolutional filters used in Network-A and Network-B  
(a) Global descriptor extraction process by Network-A (b) Diffused descriptor extraction process by Network-B

Sample feature map obtained by Network-A and Network-B is illustrated in Fig. 8(b) and Fig. 8(c) respectively. Fig. 8(b) illustrates the global feature map, while Fig. 8(c) illustrates the diffused feature maps. When comparing the global feature map and the diffused feature map, the diffused feature map contains more information on the selected lesion candidate region. For training the suggested Py-CNN approach, the Adam optimizer with a learning rate of 0.01 is used. The training was performed with a batch size of 16 for 60 epochs.

Table III: Class-wise performance obtained by the Py-CNN-based approach for the Messidor-2 dataset

Classes	F1-score (%)	Recall (%)	Specificity (%)	MCC (%)	Precision (%)	Accuracy (%)
SeNPDR	94.51	95.56	99.39	94.00	93.48	95.56
MoNPDR	97.01	96.01	98.79	95.16	98.04	96.02
MiNPDR	96.81	96.71	98.67	95.43	96.91	96.71
PDR	82.09	87.30	98.97	81.47	77.46	87.30
Healthy	97.55	98.03	99.31	96.98	97.08	98.03

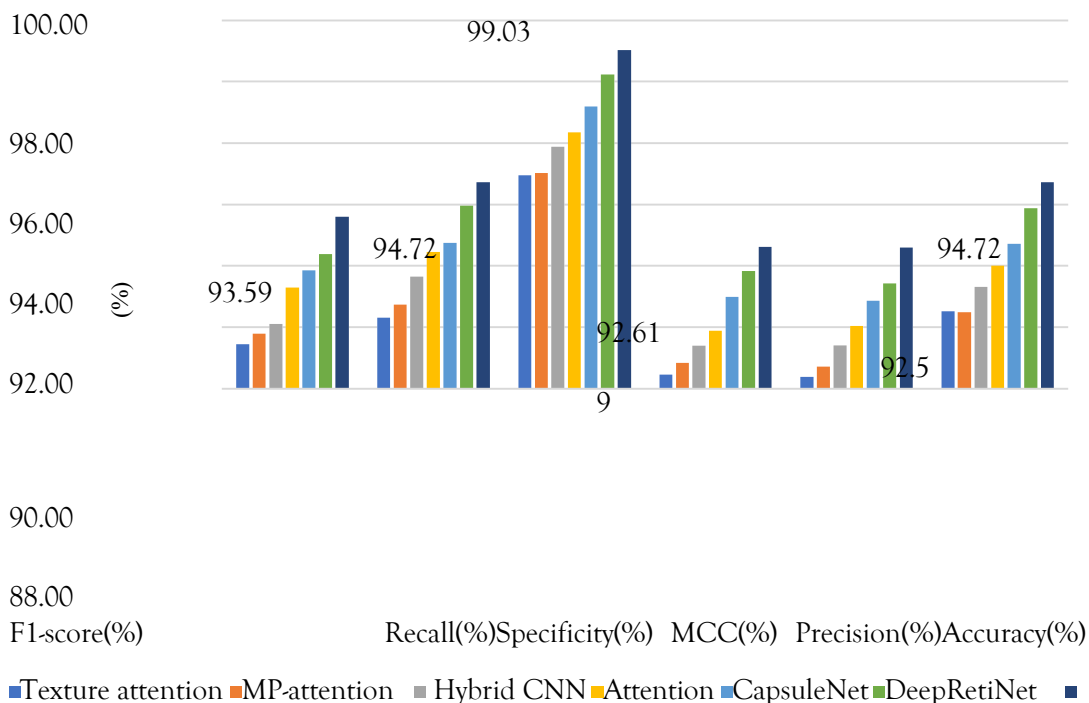
Table III provides the class-wise comparison of performance using the suggested Py-CNN approach when analyzed utilizing the Messidor-2 dataset. For the classes SeNPDR, MoNPDR, MiNPDR, PDR, and Healthy cases, the Py-CNN provides an accuracy of 95.56%, 96.02%, 96.71%, 87.30%, and

98.03% respectively when evaluated using the Messidor-2 dataset. The classification accuracy is maximum for the class healthy, while it is lower for the PDR cases. The performance of the proposed Py-CNN-based DR severity grading approach was compared with other DR severity grading approaches namely texture attention [29], MP-attention [30], Hybrid CNN [31], attention [16], CapsuleNet [17], and DeepRetiNet [14] approaches as provided in Table IV.

Table IV: Performance comparison between the suggested Py-CNN-based DR grading approach and other approaches when evaluated using the Messidor-2 dataset

Schemes	F1-score (%)	Recall (%)	Specificity (%)	MCC (%)	Precision (%)	Accuracy (%)
Textureattention[29]	89.45	90.31	94.96	88.46	88.38	90.52
MP-attention[30]	89.79	90.74	95.02	88.84	88.72	90.49
HybridCNN[31]	90.10	91.65	95.88	89.39	89.41	91.31
Attention[16]	91.30	92.45	96.35	89.88	90.04	91.99
CapsuleNet[17]	91.86	92.75	97.19	90.98	90.87	92.72
DeepRetiNet[14]	92.39	93.96	98.24	91.83	91.43	93.88
Proposed	93.59	94.72	99.03	92.61	92.59	94.72

For the suggested Py-CNN approach the F1-Score, recall, specificity, MCC, precision, and accuracy were estimated as 93.59%, 94.72%, 99.03%, 92.61%, 92.59%, and 94.72% respectively. When comparing the suggested Py-CNN with the DeepRetiNet approach, the F1- score, recall, specificity, MCC, precision, and accuracy improve by 1.2%, 0.77%, 0.79%, 0.78%, 1.17%, and 0.84% respectively when evaluated using the Messidor-2 dataset. The graphical comparison is provided in Fig. 9.



## Proposed

Fig. 9: Graphical comparison of performance between suggested Py-CNN and similar DR grading schemes when evaluated using Messidor-2 data

The class-wise performance comparison between different DR classes when evaluated using the APTOS 2019 dataset is illustrated in Table V. In the case of the APTOS 2019 dataset, the proposed Py-CNN yields an accuracy of 97.98%, 97.78%, 97.60%, 96.05%, and 97.97% for the DR grades SeNPDR, MoNPDR, MiNPDR, PDR, and healthy respectively.

Table V: Class-wise performance obtained by the Py-CNN-based approach for the APTOS 2019 dataset

Classes	F1-score (%)	Recall (%)	Specificity (%)	MCC (%)	Precision (%)	Accuracy (%)
SeNPDR	96.87	97.98	99.43	96.46	95.77	97.98
MoNPDR	97.67	97.78	98.94	96.66	97.56	97.78
MiNPDR	97.67	97.60	99.35	97.00	97.74	97.60
PDR	97.14	96.05	99.63	96.54	98.27	96.05
Healthy	97.70	97.97	99.43	97.18	97.43	97.97

The average F1-score, recall, specificity, MCC, precision, and accuracy estimated by the suggested Py-CNN is 97.41%, 97.47%, 99.36%, 96.77%, 97.35%, and 97.47% respectively when evaluated using the APTOS 2019 dataset. The average F1-score, recall, specificity, MCC, precision, and accuracy estimated by the suggested Py-CNN approach are 0.72%, 0.58%, 0.57%, 0.79%, 0.45%, and 0.52% respectively when evaluated using the APTOS 2019 dataset.

Schemes	F1-score (%)	Recall (%)	Specificity (%)	MCC (%)	Precision (%)	Accuracy (%)
Textureattention[29]	93.67	93.63	95.67	92.66	93.49	93.48
MP-attention[30]	93.88	94.06	95.85	93.15	93.94	94.09
HybridCNN[31]	94.82	94.60	96.69	93.99	94.31	94.51
Attention[16]	95.23	95.54	97.38	94.81	95.17	95.42
CapsuleNet[17]	95.96	96.22	98.00	95.69	95.89	96.06
DeepRetiNet[14]	96.68	96.90	98.79	95.98	96.90	96.95
Proposed	97.41	97.47	99.36	96.77	97.35	97.47

Table VI: Performance comparison between the suggested Py-CNN-based DR grading approach and other approaches when evaluated using the APTOS 2019 dataset

The graphical comparison of performance between the suggested Py-CNN approach and other similar schemes when evaluated using the APTOS 2019 dataset is presented in Fig. 10. The comparison shows that the performance of the suggested scheme is higher than other approaches used for comparison.



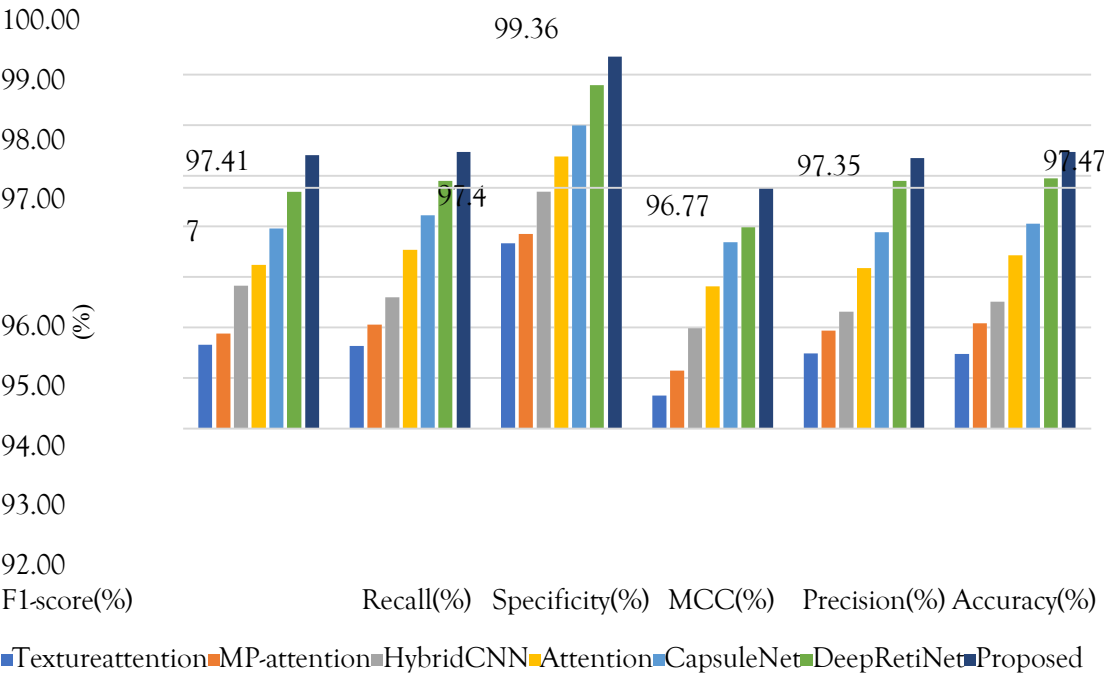


Fig. 10: Graphical comparison of performance between suggested Py-CNN and similar DR grading schemes when evaluated using APTOS 2019 data

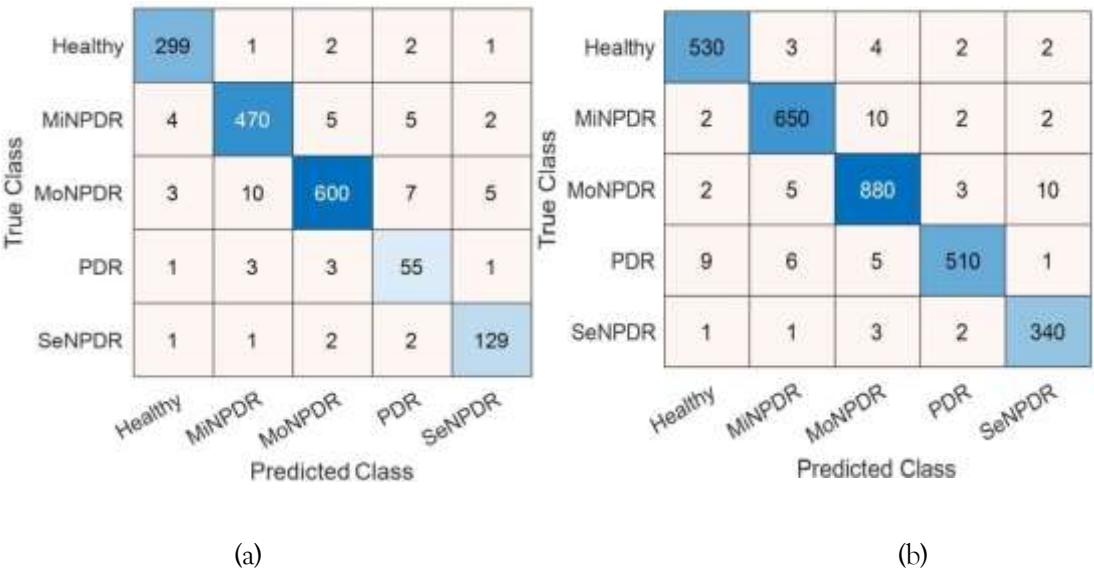




Fig. 11: Confusion matrix estimated during the testing phase of Py-CNN model (a) Messidor-2  
(b) APTOS 2019 dataset

The confusion matrix obtained by the suggested Py-CNN during the testing process utilizing the Messidor-2 and APTOS 2019 is illustrated in Fig. 11(a) and Fig. 11(b) respectively. When comparing the two datasets, the APTOS 2019 dataset provides a higher proportion of true positives than the Messidor-2 dataset. This shows that the suggested approach provides higher performance for the APTOS 2019 dataset than the Messidor-2 dataset.

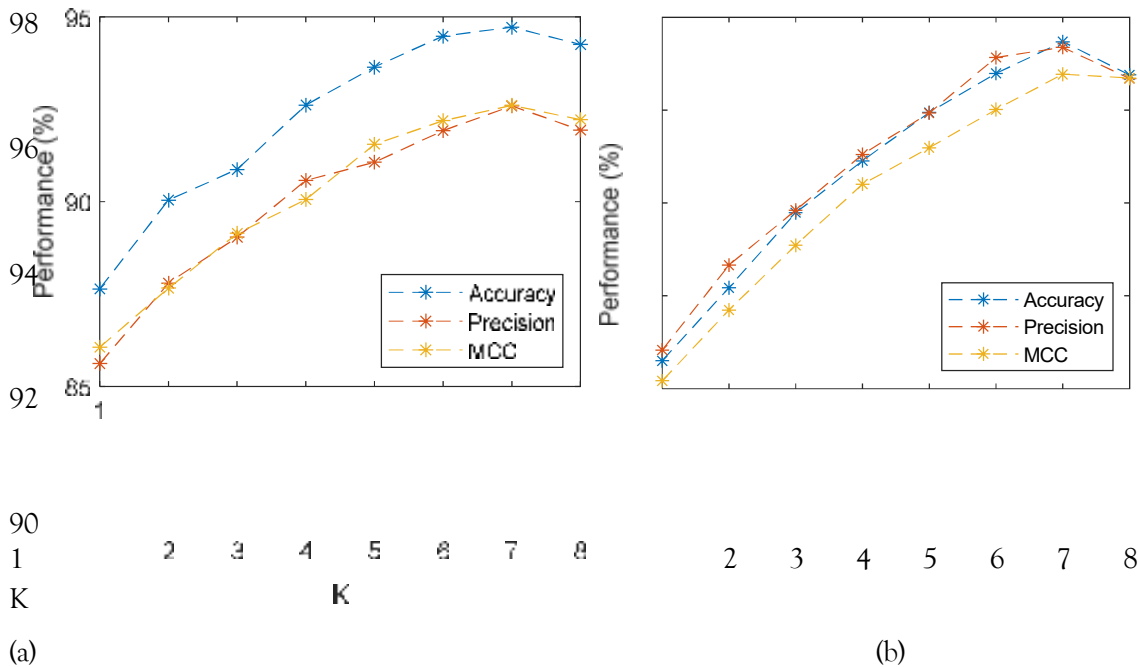


Fig. 12: Variation of performance with respect to the parameter (a) Messidor-2 (b) APTOS 2019 dataset

The variation of measures such as accuracy, precision, and MCC with respect to  $K$  is provided in Fig. 12. As the  $K$  value increases from 1, the performance increases. The performance attains maximum with  $K = 7$ . This resembles that the usage of more lesion candidates extracts more deep features. For further increases in  $K$  value, the performance is slightly reduced. This reduction is due to the increase in redundant features or due to the involvement of normal regions in the extraction of deep features.

#### 4. CONCLUSION

The work proposed a Pyramidal structured convolution-based (Py-CNN) DR grading approach that uses a rank-based lesion candidate estimation. The scheme initially preprocesses the fundus image to enhance the DR lesion candidate's region. The DR lesion candidates are then segmented and a rank is computed for each candidate. The Py-CNN structure has the pyramidal structure of convolutional filters, where features are extracted from the top-ranked candidates using a convolutional filter having a larger length. As the rank reduces, the filter length also reduces. Features such as diffused features, lesion candidate features, and global features are extracted using the Py-CNN. Two dense networks are used in the Py-CNN classifier, where the first dense network uses the combined features namely the global feature and the candidate feature, while the second dense network uses the diffused

features. The actual predicted probability is estimated from the average probability of the two dense networks to classify the DR grades such as PDR, healthy, and NPDR types (Severe, mild, and moderate). Publicly available DR grading datasets such as Messidor-2 and APTOS 2019 are utilized for evaluating the Py-CNN classifier performance. The proposed Py-CNN classifier provides an accuracy of 94.72% and 97.47% when evaluated using the Messidor-2 and APTOS 2019 datasets.

## REFERENCES

- [1] Fong, D. S., Aiello, L. P., Ferris III, F. L., & Klein, R. (2004). Diabetic retinopathy. *Diabetes care*, 27(10).
- [2] Stitt, A. W., Curtis, T. M., Chen, M., Medina, R. J., McKay, G. J., Jenkins, A., ... & Lois, N. (2016). The progress in understanding and treatment of diabetic retinopathy. *Progress in retinal and eye research*, 51, 156-186.
- [3]. Vujosevic, S., Aldington, S. J., Silva, P., Hernández, C., Scanlon, P., Peto, T., & Simó, R. (2020). Screening for diabetic retinopathy: new perspectives and challenges. *The Lancet Diabetes & Endocrinology*, 8(4), 337-347.
- [4]. Kollias, A. N., & Ulbig, M. W. (2010). Diabetic retinopathy: early diagnosis and effective treatment. *Deutsches Arzteblatt International*, 107(5), 75.
- [5]. Suchetha, M., Ganesh, N. S., Raman, R., & Dhas, D. E. (2021). Region of interest-based predictive algorithm for subretinal hemorrhage detection using faster R-CNN. *Soft Computing*, 25(24), 15255-15268.
- [6]. Wan, S., Liang, Y., & Zhang, Y. (2018). Deep convolutional neural networks for diabetic retinopathy detection by image classification. *Computers & Electrical Engineering*, 72, 274-282.
- [7]. Krishnan, S. H., Vishwa, C., Suchetha, M., Raman, A., Raman, R., Sehastrajit, S., & Dhas, D. E. (2023). Comparative performance of deep learning architectures in classification of diabetic retinopathy. *International Journal of Ad Hoc and Ubiquitous Computing*, 44(1), 23-35.
- [8]. Qummar, S., Khan, F. G., Shah, S., Khan, A., Shamshirband, S., Rehman, Z. U., ... & Jadoon, W. (2019). A deep learning ensemble approach for diabetic retinopathy detection. *Ieee Access*, 7, 150530-150539.
- [9]. Kalyani, G., Janakiramaiah, B., Karuna, A., & Prasad, L. N. (2023). Diabetic retinopathy detection and classification using capsule networks. *Complex & Intelligent Systems*, 9(3), 2651-2664.
- [10]. Kar, S. S., & Maity, S. P. (2017). Automatic detection of retinal lesions for screening of diabetic retinopathy. *IEEE Transactions on Biomedical Engineering*, 65(3), 608-618.
- [11]. Wang, Z., Yin, Y., Shi, J., Fang, W., Li, H., & Wang, X. (2017). Zoom-in-net: Deep mining lesions for diabetic retinopathy detection. In *Medical Image Computing and Computer Assisted Intervention—MICCAI 2017: 20th International Conference, Quebec City, QC, Canada, September 11-13, 2017, Proceedings, Part III* 20 (pp. 267-275). Springer International Publishing.
- [12]. Das, S., Kharbanda, K., Suchetha, M., Raman, R., & Dhas, E. (2021). Deep learning architecture based on segmented fundus image features for classification of diabetic retinopathy. *Biomedical Signal Processing and Control*, 68, 102600.
- [13]. Qiao, L., Zhu, Y., & Zhou, H. (2020). Diabetic retinopathy detection using prognosis of microaneurysm and early diagnosis system for non-proliferative diabetic retinopathy based on deep learning algorithms. *IEEE Access*, 8, 104292-104302.
- [14]. Chellaswamy, P., & Kamalam, C. J. R. N. R. (2025). Attention-enhanced Deep RetiNet for robust hard exudates detection in diabetic retinopathy. *Biomedical Signal Processing and Control*, 100, 106903.
- [15]. Navaneethan, R., & Devarajan, H. (2024). Enhancing diabetic retinopathy detection through preprocessing and feature extraction with MGA-CSG algorithm. *Expert Systems with Applications*, 249, 123418.
- [16]. Romero-Oraá, R., Herrero-Tudela, M., López, M. I., Hornero, R., & García, M. (2024). Attention-based deep learning framework for automatic fundus image processing to aid in diabetic retinopathy grading. *Computer Methods and Programs in Biomedicine*, 249, 108160.
- [17]. Oulhadj, M., Riffi, J., Khodriss, C., Mahraz, A. M., Yahyaoui, A., Abdellaoui, M., ... & Tairi, H. (2024). Diabetic retinopathy prediction based on vision transformer and modified capsule network. *Computers in Biology and Medicine*, 175, 108523.
- [18]. Usman, T. M., Saheed, Y. K., Ignace, D., & Nsang, A. (2023). Diabetic retinopathy detection using principal component analysis multi-label feature extraction and classification. *International Journal of Cognitive Computing in Engineering*, 4, 78-88.
- [19]. Bilal, A., Zhu, L., Deng, A., Lu, H., & Wu, N. (2022). AI-based automatic detection and classification of diabetic retinopathy using U-Net and deep learning. *Symmetry*, 14(7), 1427.
- [20]. Vives-Boix, V., & Ruiz-Fernández, D. (2021). Diabetic retinopathy detection through convolutional neural networks with synaptic metaplasticity. *Computer Methods and Programs in Biomedicine*, 206, 106094.
- [21]. Kamble, V. V., & Kokate, R. D. (2020). Automated diabetic retinopathy detection using radial basis function. *Procedia Computer Science*, 167, 799-808.
- [22]. Pao, S. I., Lin, H. Z., Chien, K. H., Tai, M. C., Chen, J. T., & Lin, G. M. (2020). Detection of diabetic retinopathy using bichannel convolutional neural network. *Journal of Ophthalmology*, 2020(1), 9139713.

- [23]. Aziz, T., Charoenlarnnopparut, C., & Mahapakulchai, S. (2023). Deep learning-based hemorrhage detection for diabetic retinopathy screening. *Scientific Reports*, 13(1), 1479.
- [24]. Zago, G. T., Andreão, R. V., Dorizzi, B., & Salles, E. O. T. (2020). Diabetic retinopathy detection using red lesion localization and convolutional neural networks. *Computers in biology and medicine*, 116, 103537.
- [25]. Setiawan, A. W., Mengko, T. R., Santoso, O. S., & Suksmono, A. B. (2013, June). Color retinal image enhancement using CLAHE. In *International conference on ICT for smart society* (pp. 1-3). IEEE.
- [26]. Ganguly, S., Ganguly, S., Srivastava, K., Dutta, M. K., Parthasarathi, M., Burget, R., & Riha, K. (2014, November). An adaptive threshold based algorithm for detection of red lesions of diabetic retinopathy in a fundus image. In *2014 International Conference on Medical Imaging, m-Health and Emerging Communication Systems (MedCom)* (pp. 91-94). IEEE.
- [27]. Abramoff, M. D., Folk, J. C., Han, D. P., Walker, J. D., Williams, D. F., Russell, S. R., ... & Niemeijer, M. (2013). Automated analysis of retinal images for detection of referable diabetic retinopathy. *JAMA ophthalmology*, 131(3), 351-357.
- [28]. Karthik, Maggie, and Sohler Dane. APTOS 2019 Blindness Detection. <https://kaggle.com/competitions/aptos2019-blindness-detection>, 2019. Kaggle.
- [29]. Alahmadi, M. D. (2022). Texture attention network for diabetic retinopathy classification. *IEEE Access*, 10, 55522-55532.
- [30]. Zhang, C., Chen, P., & Lei, T. (2023). Multi-point attention-based semi-supervised learning for diabetic retinopathy classification. *Biomedical Signal Processing and Control*, 80, 104412.
- [31]. Ali, G., Dastgir, A., Iqbal, M. W., Anwar, M., & Faheem, M. (2023). A hybrid convolutional neural network model for automatic diabetic retinopathy classification from fundus images. *IEEE Journal of Translational Engineering in Health and Medicine*, 11, 341-350.